IMPRS NeuroCom

Microscopical Imaging in Neuroscience

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The basics:

Seeing! Determined by the "resolving power", the smallest distance between neighboring pixels that can be perceived separately. The resolution is limited by the angle that two rays form in the eye that hit adjacent photoreceptors.

The resolving power can be increased by changing the angle, under which an object appears.

This can be achieved on the one hand by approaching the eye



or by optical aids, e.g. through "microscopes / lenses" of all kinds.



MICROSCOPY

<u>Greek</u>

mikro = small

skopien = to observe

"To observe small things"

Principle of the light microscope:



Eye or camera

virtual, right-sided, magnified image

Eyepiece as a magnifying glass (2. magnification)

Intermediate image

real, inverted, magnified image

Lens (1. magnification, variable)

Specimen

Condenser

Illumination with aperture

Light microscopic techniques:

Brightfield microscopy: Different absorption of light

Dark field microscopy: No direct light in the lens-sample, stray light, Tyndall effect



Polarizing microscopy: Different indices of refraction of light. It is used to examine optically anisotropic (birefringent) objects.

Brightfield





Light microscopic techniques:

Contrast microscopy:

Contrast-enhancing procedures that deliver highcontrast images of transparent, unstained specimens

Phase contrast microscopy (Ph1-3):

Differences in the density of structures are shown.

Differential interference contrast (DIC):

Similar to phase contrast, differences in the density of structures are made visible. Advantages compared to the phase contrast: offers sufficient contrast even with high resolution.





Köhler Illumination

Through Koehler illumination arrangement a uniformly illuminated image field is achieved without the image of the light source in the specimen plane. In addition, by centering the light source one achieves a maximum light output, which is of great importance especially for the contrast method.



Resolution and magnification:

A higher magnification does not automatically go hand in hand with a higher resolution.



The **resolving power** is mainly represented by the **numerical aperture** of the objective.



Higher magnification with the same resolution, the picture appears blurry and details are not resolved.

numerical aperture(NA) <u>NA = n sin α </u>

n = Refractive index of the medium (between specimen and objective)

 α = half the opening angle of the lens





Depth of field (imaging depth / depth of field) (DOF):

DOF = $n \times \lambda / 2x (NA)^2$

n = refractive index of the medium (between specimen and objective)

The imaging depth describes the layer thickness in the object, in which this appears sharp (depth of focus / depth of field). The **higher the NA** of the lens, the the **smaller the depth of field** / imaging depth in the object



Unschärfekreis
 Schärfentiefe

Important indices of refraction

Vacuum:	1
Air:	1,0003
Water:	1,33
Glass:	1,4 - 1,8
Cover slip:	1,513



Immersion media:

Immersion oil:	1,516
Canada balm:	~1,52
Epoxyd resin:	~1,56



Lenses (labeling) and tube length:



PlanC N (Objektivserie, Objektivklasse(Planachromat))
20x / 0.40 (Magnification/ numerical aperture)
∞ / 0.17 (Tube length / cover glass thickness)
/ FN 22 (Field of view (Field Number))



Field of View (FOV) and Field Number (FN):

FOV = Field Number (FN) / Objective Magnification = 22 / 20 = 1,1 mm





Resolution (d) and Abbe diffraction limit:

 λ = wavelength of the light used NA = numerical aperture of the objective



So e.g. light with 500nm with a 20x, 40x or 63x objective with an NA of 1.0 results in a resolution of 250nm (~roughly the diffraction limit, means I can distinguish between two points that are 250nm apart), it doesn't matter whether I use 20x, 40x, 63x objective !!!

Resolution of 250nm only applies "in plane" x-y direction.

The z-direction has a poorer resolution by a factor of ~2-4 (500-1000nm)



The resolution (d) is disturbed by various imaging errors

Chromatic aberration Spherical aberration

and by diffraction of light

Due to the wave properties of light, the real behavior deviates strongly from what one would expect



Point spread function (PSF)



Deconvolution



https://svi.nl/Huygens-Deconvolution

Brightfield Microscopy

Standard light microscopic systems

Zeiss Axiophot with RGB AxioCam HRC Camera





Files size around 4-8 MB

FOV, even with the most expensive 2,5x objective with **0.1 NA**, is just around **20mm** and you have a resolution of ~**2-3mm**.



Digital Automated Microscopy



Zeiss AxioScan.Z1 Automated Microscope available since 2017/18

Digital Automated Microscopy

Myelin Basic Protein Antibody







Serial cut recording with the Zeiss AxioScan.Z1 microscope 100 slides (76x26mm)

50 slides (76x52mm)

25 slides (102x76mm)

Resolution 250-1000nm x-y approx. 1 μ m in the z direction Z-stacks with EDF (Extended Depth of Focus) and MIP (Multi Image Projection)

Light microscopy

Fluorescence microscopy DAPI, Cy2, Cy3, Cy5 and Cy7 Objectives 5x (NA 0.25), 10x (NA 0.45), 20x (NA 0.5), 20x (NA 0.8), and 40x (NA 0.95)

Recording speed ~ 2cm² per minute with 20x objective Price approx. 200,000 Euros



Switch to Zeiss ZEN

Epi-Fluorescence Microscopy

Principle of fluorescence microscopy:

Excitation = short wave length Emission = long wave length



Light source: HBO, HPX Colibri LED



Excitation filter
 (allows light of the excitation wavelength (s) to pass)
 Dichroic mirror

(breaks excitation light, lets emission light pass)

3. Emission filter

(specifically lets the emission light pass)

Epi-Fluorescence Microscopy

Epi-Fluorescence microscopic system

Zeiss Axioscope with monochrome AxioCam ICm





Images taken at 2,5x (0.05 NA), 10x (0.3 NA) and 40x (1.2NA)

Files size around 2-6 MB





Widefield Illumination

Widefield Detector

Objective

Sample

Condenser

Widefield Light source Image = In-focus + Defocus PSF's

<u>Pro's</u>

• Many points are imaged simultaneously, increasing the image capture speed

<u>Con's</u>

- Out of focus light reduces the contrast of the image
- Out of focus excitation leads to excessive photo damage

Principle of CLSM (Confocal Laser Scanning Microscope):





LSM 880-NLO Fast Airyscan



Pinhole vs Airyscan

Confocal imaging with pinhole at 1 AU





Airyscan

Confocal imaging with Airyscan





Airyscan processing / detector deconvolution and spatial assignment



Airyscan

Superresolution and Sensitivity at Speed



Airyscan / new confocal imaging



~80-120 nm lateral resolution with a single image



Airyscan / highSNR and high Speed



Standard Scanner – **40-80 FPS**



Airyscan Mode – 96 FPS

- Resolution: ~ 2-3x
- Speed: 2-3x
- Signal to noise: 4x

Cardiomyocyte Cells with tubulin-EMTB to measure microtubule buckling Images and Samples Courtesy of Ben Prosser, UPENN – "Detyrosinated microtubules buckle and bear load in contracting cardiomyocytes", Science April 2016

Point Scanning Confocal Illumination



Image = In-focus PSF's only

<u>Pro's</u>

• Out of focus light does not obscure the contrast of the image

<u>Con's</u>

- One point is imaged at a time, meaning image collection is slow.
- Out of focus excitation leads to excessive photodamage
- Photon efficiency is reduced by the need for a pinhole

Switch to Zeiss ZEN

Conventional Illumination

Both widefield and confocal microscopy induce significant photobleaching/photo-toxicity during 3D image acquisition



Orthogonal plane imaging | Selective Plane illumination Microscopy

- First described by Siedentopf and Zsigmondy in 1903
- First used for fluorescence imaging by Voie et al., in 1994
- The term SPIM was coined by Huisken et al., in 2004



SPIM Sample Viewing



SPIM Inverted Selective Plane Illumination



Marianas Lightsheet | University of Leipzig, PFI-System



Marianas Lightsheet | Imaging Modes - diSPIM

Piezo/Slice Scanning: Dual acquisition of image stacks using a coordinated movement of the slice position and the piezo. One volume from each side.



Marianas Lightsheet

Resolution of 40x 0.8NA objectives, with a sheet thickness of 3µm



Scale of Sample

